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Digestive Activity Evaluation by Multichannel Abdominal Sounds Analysis

Radu Ranta*, *Member, IEEE*, Valérie Louis-Dorr, Christian Heinrich, Didier Wolf, and François Guillemin

Abstract—This paper introduces a complete methodology for abdominal sounds analysis, from signal acquisition to statistical data analysis. The goal is to evaluate if and how phonoenterograms can be used to detect different functioning modes of the normal gastrointestinal tract, both in terms of localization and of time evolution during the digestion. After the description of the acquisition protocol and the employed instrumentation, several signal processing steps are presented: wavelet denoising and segmentation, artifact suppression, and source localization. Next, several physiological features are extracted from the processed signals issued from a database of 14 healthy volunteers, recorded during 3 h after a standardized meal. Data analysis is performed using a multifactorial statistical method. Based on the introduced approach, we show that the abdominal regions of healthy volunteers present statistically significant phonoenterographic characteristics, which evolve differently during the normal digestion. The most significant feature allowing us to distinguish regions and time differences is the number of recorded sounds, but important information is also carried by sound amplitudes, frequencies, and durations. Depending on the considered feature, the sounds produced by different abdominal regions (especially stomach, ileocaecal, and lower abdomen regions) present a specific distribution over space and time. This information, statistically validated, is usable in further studies as a comparison term with other normal or pathological conditions.

Index Terms—Abdominal sounds, digestion evolution, factorial analysis, wavelet denoising.

I. INTRODUCTION

ONE of the oldest means of physiological investigation, still currently used in clinical routine, is the auscultation. The instrumentation is simple (stethoscope), and its utility is largely recognized especially for cardiac and pulmonary sounds.

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Relatively little studied for abdominal sounds, although the first papers appeared a century ago [1], the phonoenterography presents significant potentialities [1]–[8]. Different applications can be imagined, from the study of the normal physiology (classifying digestion phases or abdominal regions) to clinical routine (functional diseases diagnostic aid and postsurgical monitoring) or pharmacological research (medication effect on the gastrointestinal activity).

Two types of approaches for phonoenterogram interpretation are proposed in the literature: the first one focuses on the analysis of individual sounds, classified, for example, in 1°, 2°, and 3° sounds [9], clicks, multiclicks and complexes [3], intestinal bursts, and regularly sustained sounds [10]. The second approach, adopted here, is more widely used and tries to analyze sequences of phonoenterograms using different, so called, “activity indexes” like mean sound duration, silence between sounds duration, signal energy, etc. The underlying hypothesis is that abdominal sounds, recorded upon long periods of time and in several abdominal locations, are representative of the physiological activity, either normal or pathological. Under this hypothesis, changes in the patient status are reflected in the activity indexes, which can be used to assess and quantify differences among normal or pathological physiological states [2], [5], [6], [11]–[13]. However, phonoenterogram interpretation is particularly difficult: There is no consensus on a method for processing and analyzing abdominal sounds over long durations and in simultaneous locations (see the comparative studies [14] or [15]).

The first goal of this paper is to propose a complete (although not unique) signal acquisition, processing, and analysis methodology, able to extract significant activity indexes from long-term multichannel phonoenterograms. The second and more important goal is to use these indexes to analyze the influence of the physiological factors, such as the patient, the abdominal region, and the digestion phase, on the phonoenterograms. A detailed statistical analysis is performed to check if phonoenterograms, characterized by simple physiological activity indexes, can be used to make statistically valid affirmations about the digestion: which regions can be distinguished, when, how much time one has to record (listen), and which are the indexes that can be used to make this difference.

We focus here only on the digestion of the healthy volunteers, in order to obtain a phonoenterographic point-of-view description of the normal functioning of the digestive tract, in the given controlled recording conditions. The obtained spatial–temporal (regions–digestion phases) distribution of the abdominal activity is statistically validated through a nonparametric factorial data analysis (analysis of variance (ANOVA) type) and can constitute

a comparison term for other normal or pathological phonoenterogram data, recorded and extracted in similar conditions.

After this introduction, the second section describes the signal acquisition and processing methods. The main addressed issues are the protocol used to ensure the repeatability of the measures and the novelties introduced in the denoising procedure. The next section presents the experimental design and the statistical analysis methods. Section IV details and discusses the results and is followed by a conclusion and by possible future research directions.

II. SIGNAL ACQUISITION AND PROCESSING

This paper uses similar acquisition protocol and instrumentation as our previous works [12], [13], [16]–[18]; therefore, we focus on the test protocol used to ensure the repeatability of the measures. Moreover, as most of the employed signal processing methods were already introduced and validated in the cited papers, only a brief reminder is presented here.

A. Rationale

Regardless of the data analysis methodology, the obtained results are influenced by the elements of the acquisition and signal processing chain. To reduce the possible variations of the activity indexes due to the acquisition,¹ we place ourselves in a controlled environment (identical instrumentation, recording conditions, and signal processing for all recording channels and all patients). These conditions must, of course, deal with phonoenterogram difficulties, which are as follows.

- 1) Long-term recordings have a high variability, either in time (digestion phases), location (abdominal region), or among patients. For a valid interpretation, it is necessary to record on several patients, in different abdominal locations and using similar recording conditions (standardized protocol and instrumentation).
- 2) Individual abdominal sounds have a highly irregular character and random appearance (although quasi-periodic bursts have already been detected by Cannon [1], a century ago), and they are contaminated by noise and artifacts (movements, heart beats, etc.). It is then necessary to detect, segment, and denoise them, as well as to characterize them in order to eliminate the artifacts.

B. Data Acquisition

1) *Experimental Protocol*: Our database consists of 14 healthy volunteers of medium build, partially based upon the dataset used in [13].² All phonoenterograms were recorded in similar conditions and, to avoid perturbing the normal digestion of the volunteers, the choice of the meal was adapted to their alimentary habits: a standardized breakfast was taken at about 8:30 a.m. and consisted in a cup of tea/coffee, two bread rolls, 200 mL of orange juice, and one yoghurt. The end of

¹Real clinical auscultation conditions can be highly variable and they could influence the results of the analysis.

²Compared to [13], some patients were eliminated and others were added to obtain an homogeneous database.

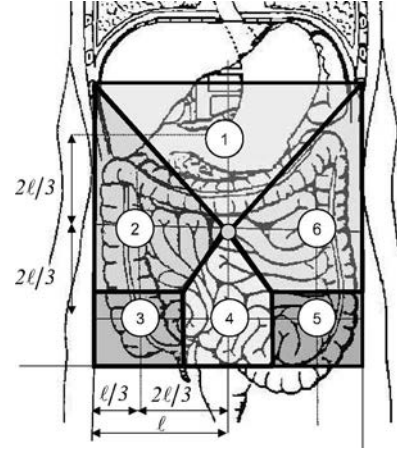


Fig. 1. Stethoscope placement and abdominal regions: ℓ stands for the distance between the navel and the lateral side.

the recording, almost 3 h later (168 min), is very close to the main meal of the day, taken at about 12:00, and therefore, we consider that we can follow the digestion (postprandial period) and have the “hungry” period (preprandial) for each volunteer. A completely lied-down position (which could be more appropriate for good recording conditions) was difficult to accept and maintain for the whole recording duration, and therefore, the volunteers’ position was halfway between lying and sitting so they could watch television (using a headset to avoid phonoenterogram contamination by the TV sound). In order to minimize movement artifacts, they were instructed not to change their position during the recording.

2) *Acquisition Sites*: To obtain local information for different abdominal regions, six recording channels (1, 2, . . . , 6) were used (see Fig. 1). In order to respect interpatient variability, channels 1, 2, 4, and 6 were positioned at equal distances from the navel. This distance was taken at two-third from the total distance between the navel and the lateral side of the abdomen. Channels 3 and 5 were aligned to channels 2, 4, and 6. These positions aim to record sounds over significant abdominal structures and cover the whole abdominal surface (1 on duodenum, 2 on the ascending colon, 3 on the ileocaecal valve, 4 on the small bowel, and 5 and 6 on the descending colon).

3) *Acquisition Instrumentation*: Most of the literature reports classic microphones for acquiring abdominal sounds (as, for example, in [1], [2], [4], [5], and [19]). Commercial electronic stethoscopes were used by Craine *et al.* [6], [7]. We have followed the approach of Garner and Ehrenreich [3], who adapted electret microphones to classic stethoscope heads. The six sensors were fixed on the abdomen wall with an elastic band.

Obviously, to these sensors, we associated conventional analog electronics containing adjustable voltage amplifiers and bandpass antialiasing filters, calibrated to the bandwidth of the A/D converter (Nicolet Vision 8 channels digital acquisition system, 16 bits resolution). According to the frequency characteristics of the signal (band-limited between 100 and 500 Hz, see next paragraph), the chosen sampling frequency was 5000 Hz.

The advantage of this instrumentation choice is that it allows a perfect control of the acquisition parameters: the six channels

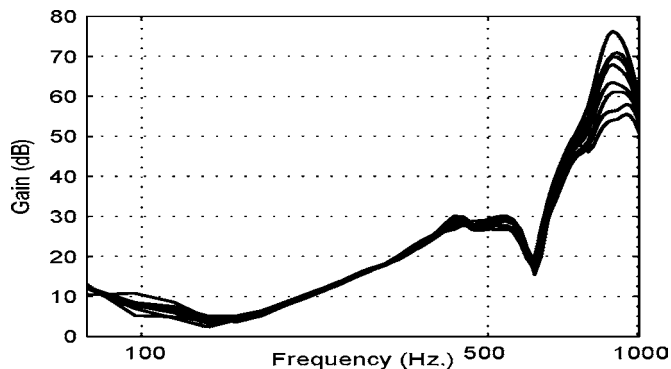


Fig. 2. Superimposed frequency responses for different sensor pressures varying from 390 to 3510 Pa (with a step of 390 Pa), corresponding to masses between 0.05 and 0.4 kg (0.05 kg step) placed on the stethoscope head.

were calibrated in the same manner, and this calibration was verified before each recording.

The developed acquisition system has its pitfalls: first, the frequency response due to the stethoscope head is not flat. Still, commercial electronic stethoscopes also present selective frequency responses, which vary considerably from one another [20]. Second and more important, the six channels might have different responses among regions and among volunteers, because of the variations in the fixation system. With this ideas in mind, we tried to evaluate, on one hand, the frequency response in the frequency band of interest and, on the other hand, the influence of the pressure applied by the stethoscope head against the patient’s abdominal wall.

The frequency responses of the sensor were evaluated for different pressures, situated in a large enough interval (≈ 400 to ≈ 3500 Pa) to cover the actual pressures of the stethoscope head on the abdominal wall during the phonoenterogram recording. Measures were done in an anechoidal chamber by pressing the stethoscope head against an abdomen phantom using different force values and a calibrated white-noise source between 100 and 1000 Hz. As expected, the frequency response of the stethoscope head is not flat, unlike the frequency response of the microphone alone (compared to those recorded using only the microphone, all sounds acquired through a stethoscope head are amplified from 5 to 30 dB over the band of interest 100–500 Hz, see Fig. 2). The curves presented in Fig. 2 correspond to different pressures and, as it can be seen, they are rather slightly influenced by the pressure in the frequency band 100–500 Hz, although more important variations appear for higher frequencies (around 800 Hz).

Finally, a last evaluation of the acquisition system was performed by medical expertise. Several minutes of the recorded phonoenterograms were listened to and annotated by a clinician, who confirmed the good quality of the recordings from the medical interpretation point of view.

We, therefore, conclude that the frequency response of the instrumentation does not distort the physiological information carried by the abdominal sounds. Moreover, it does not significantly vary because of the fixation system, and thus, neither among different recordings (in time or across the different re-

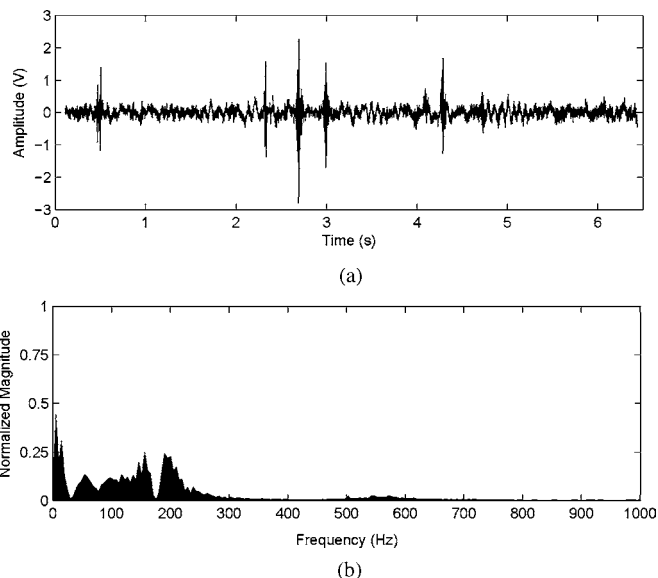


Fig. 3. Typical phonoenterogram recording. (a) Time course. (b) Spectral content (normalized to unitary energy).

gions or different patients). Therefore, no acquisition bias affects the signal analysis presented in the sequel, and comparisons among regions and patients make sense, as the recordings were performed in similar conditions.

4) *Signal*: Healthy phonoenterograms are characterized by a succession of isolated short events. The signal consists of a sparse succession of nonstationary impulsive sounds [see Fig. 3(a)]. They can appear in periodic bursts of activity (3 to 12 per min, according to the place and time of their generation) [1], [2]. The parts of the signal that separate the sounds, called in the bibliography “periods of silence,” are not actually completely quiet. Noise due to acoustic effects of the stethoscope and other low-frequency physiological sounds (breathing and blood flow) is superimposed on the informative signal and must be taken into account in any further processing.

The frequency content of the phonoenterogram is relatively poor. The literature indicates maximum frequencies of the abdominal sounds lower than 1000–1500 Hz [4], [5], [7], [21], even if other values are mentioned (5000 Hz, for example, in [3]). The principal frequency of the abdominal sounds is generally higher than the frequencies of the cardiac and pulmonary sounds, and sometimes a high-pass filtering at 80 Hz is used to eliminate the influence of the latter [5]. The frequency content of the noise is almost identical to that of the signal and cannot be eliminated by simple filtering.

The literature description of the abdominal sounds is confirmed by our observations. Their frequency content is band-limited: only approximately 0.5% of the signal energy is located beyond 1000 Hz and only approximately 2% beyond 500 Hz. In fact, almost all of the phonoenterogram energy is situated between 100 and 500 Hz [see Fig. 3(b)].

C. Denoising and Segmentation: *HystD* Algorithm

Considering the signal characteristics (sparse transients), nonstationary denoising algorithms seem to be the most

appropriate. This hypothesis was validated by our previous work and by several other authors, who developed wavelet-based algorithms for abdominal sounds denoising [13], [22]–[26]. Automatic segmentation procedures are proposed in [13], [19], and [24].

The first wavelet-denoising algorithm applied on bowel sounds was the iterative wavelet transform-based stationary-nonstationary filter (WTST-NST) proposed in [23] and derived from the “peeling algorithm” presented in [27]. We have shown in [16] and [18] that WTST-NST may be seen as a fixed-point algorithm, and we have analyzed and determined its convergence conditions by introducing generalized Gaussian (GG) modeling of the wavelet coefficients. This approach leads to a “minimal denoising” algorithm (MinD), completely parameter-free and ensuring a maximum information extraction from the measured signal. The main drawback of these methods is the fact that they tend either to overestimate the number of individual abdominal sounds (WTST-NST and MinD) or to distort the detected ones (especially WTST-NST with a different parametrization $F_a > 3$, see [26]).

Several improvements were proposed over the past years. Fractal dimension estimation in the wavelet domain was used in [25] and [28] to diminish the distortion of the detected events. Wiener filtering (in the wavelet domain also) was proposed in [26] to avoid overdetection and minimize distortion. We proposed a different approach, called “hysteresis denoising,” in [13], which achieves denoising and segmentation in the same time, ensuring also a limited distortion of the segmented events. A slightly modified version of this algorithm (5) is briefly reminded here. Comparison with other recent signal processing developments, such as those introduced in [10], [19], [25], [26], and [28], is beyond the purpose of this paper.

We consider the model $z = x + n$, where z is the noisy discrete-time signal of length N and x is the noise-free unknown version of z and n the noise. Synthetically, the orthogonal discrete wavelet transform (DWT) of z writes

$$z = \sum_{p,j} w_z^{j,p} \psi^{j,p} + \sum_p w_z^{M,p} \phi^{M,p} \quad (1)$$

where $j = [1, \dots, M]$ is the scale, $p = [1, \dots, 2^{-M}N]$ is the position, ψ is the wavelet, ϕ is the scaling function, and M is the analysis depth [29]. The denoising threshold is computed using the fixed-point iteration

$$T_{j,k+1} = F_a \sqrt{\frac{1}{N} \sum_p (w_z^{j,p} \max(0, \text{sign}(|w_z^{j,p}| - T_{j,k}))^2)} \quad (2)$$

with $T_{j,k}$ being the threshold at scale j and iteration k and F_a being a multiplicative constant. This constant is user chosen for WTST-NST or function of the estimated GG probability law of shape u followed by the wavelet coefficients for MinD (see [18] for the proof)

$$F_{am} = \sqrt{\frac{3\Gamma(1/u)}{u}} (ue)^{1/u} \quad (3)$$

with $\Gamma(t) = \int_0^\infty e^{-x} x^{t-1} dx$. This F_{am} constant (subscript m stands for minimal) insures the convergence of the algorithm

to a nonnull threshold having a low value, and thus, leading to a maximal information extraction from the measured signal (minimal distortion).

For the implementation, the shape parameter u was estimated using the absolute empirical moments m_1 and m_2 (with $m_r = \mathbb{E}[|z|^r]$, see [30] and [31]).

By slightly modifying the proposition made in [13], we introduce a correction term for F_{am} , leading to a new constant

$$F_{ao} = \max(F_{am}, K_c F_{am}) \quad (4)$$

with

$$K_c = \sqrt{\frac{4 \log N}{3\sqrt{2\pi e}}}. \quad (5)$$

It is easily verified that for $u = 2$ (Gaussian law) and $F_{ao} = \sqrt{2 \log N}$, which is the well-known universal threshold proposed by [32].

The rationale behind this modification is the following: the universal threshold is constructed to asymptotically eliminate all the (Gaussian) noise from the measured signal. To adapt it to our iterative framework and to the GG case, we propose to modify the F_{am} constant, the goal being to achieve comparable performances of noise elimination. Therefore, an iterative algorithm (2) using the F_{ao} constant (4) will lead to a high threshold value, and thus, a quasi-complete noise cancelling. Moreover, applying this threshold on the approximation scale of the wavelet decomposition (low frequency), an approximate segmentation of the signal or, more precisely, a detection of the impulsive abdominal sounds, is also obtained. The price to pay for this high threshold is the distortion of the detected sounds (see Figs. 4 and 5). It is then natural to combine the two iterative algorithms in one hysteresis denoising algorithm (HystD): a high threshold (obtained with F_{ao}) to detect the greatest coefficients of each scale, and a low threshold (obtained with F_{am}) to select the “big enough” coefficients located in the neighborhood of those selected by F_{ao} .

A similar method was successfully applied in [13], and therefore, we only give some illustrative examples in Figs. 4 and 5. As it can be seen in Fig. 4, the HystD algorithm detects almost all of the individual abdominal sounds (the sixth one, undetected, was hardly hearable by the expert, but it was confirmed after several listenings). Classic iterative WTST-NST detected it, but it also detected many parasite sounds that, on one hand, confused the expert and, on the other hand, made the segmentation almost impossible (and thus, also the artifact elimination and the multichannel processing, which are partly based on the characteristics of the segmented sounds). Nevertheless, eliminating some of the sounds (as long as it remains marginal and similar for all recordings) does not influence the relative comparisons among regions and time sequences, although it might shift the absolute values.

Another situation can be observed for the first-detected sound, which visually seems distorted. A close examination of its time course and spectral content reveals that the denoising/segmentation procedure eliminated the low-frequency components (below 30 Hz, in fact), which are quite energetic. The

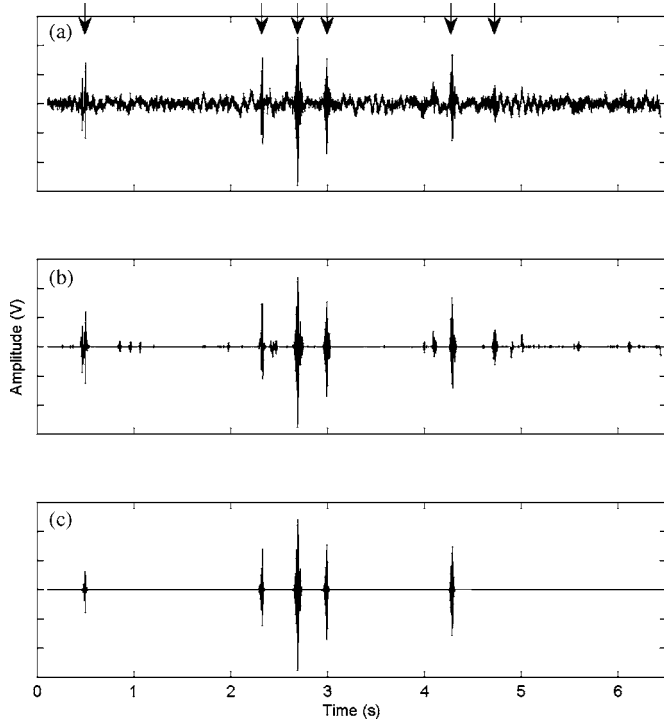


Fig. 4. (a) Example of 6.5 s of phonoenterogram. (b) Its denoised version using WTST-NST ($F_a = 3$) and (c) using novel HystD thresholding. Expert identified events are indicated by arrows.

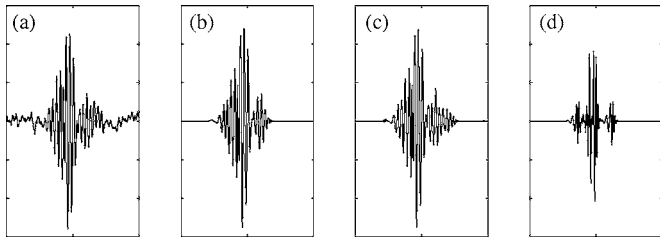


Fig. 5. Distortion comparison. (a) Example of an abdominal sound. (b) Its denoised version using WTST-NST ($F_a = 3$), (c) using HystD, and (d) using an iterative fixed-point algorithm (2) with F_{a0} (4).

auditive impression confirms this analysis: almost no difference can be heard among the three denoised versions and the original sound, except for the background noise (original signal) or a succession of parasite clicks (WTST-NST).

Although not presented in Fig. 4, the iterative thresholding using F_{a0} (4), as well as the universal thresholding, furnished denoised estimated signals visually similar to the one obtained by HystD (easy to segment, and thus, facilitating the number of sounds counting). Still, a detailed examination of the result (see Fig. 5 for a zoom on the third-detected abdominal sound in the example) shows that physiological characteristics of the sounds (amplitude, frequency, and duration) might be distorted by a too high threshold. Therefore, having in mind that our goal is to extract activity indexes from long-time recordings, a good compromise was offered by the HystD algorithm.

D. Artifact Elimination and Multichannel Processing

1) *Artifact Elimination*: Before proceeding to the multichannel processing, we have decided to heuristically eliminate remaining artifacts. Although less sensitive than WTST-NST, HystD (as certainly no denoising method) cannot ensure complete elimination of undesirable perturbations. In fact, noise cancelling methods deal with stationary noise, but noninformative (from a phonoenterographic point of view) signals are not treated. Indeed, heart beats, patient movements, and cough can be considered as informative events by the wavelet denoising/segmentation algorithm, and this kind of events are unfortunately unavoidable in long-time measurements. We have therefore introduced *a priori* knowledge at this stage of our abdominal sound processing method. For each segmented event, we have computed the most popular physical features: the duration, the energy, and the frequency spectrum, as in [4]–[7]. To avoid windowing effects, these characteristics were computed from the wavelet decomposition: duration as the union of the wavelet supports, the energy as the squared sum of the wavelet coefficients, and the frequency spectrum as the sum of the wavelet spectra. The events that did not fit the literature description of an abdominal sound were eliminated: sounds shorter than 20 ms (like hair and skin friction on the stethoscope membrane), longer than 5 s (movements), or having more than half of their energy below 80 Hz (like heart beats and respiration). On real signals, several tests showed that this approach was more effective than high-pass filtering or even adaptive filtering (with a reference stethoscope placed on the chest, for heart, cough, or movement detection).

2) *Multichannel Processing*: There are two steps of multichannel processing (see Fig. 1 for stethoscope placement). The first one concerns artifact elimination by cross-validation. In fact, we assumed that real abdominal sounds propagate inside the abdomen. Therefore, we have eliminated all sounds that are not quasi-simultaneously acquired by at least two stethoscopes (i.e., their time supports are strictly disjoint).

The second step is the localization technique. We have discussed different methods in [17]. In fact, very few publications present a multichannel approach, and most of those who do it (like [5], for example) treat the recordings in a completely independent and parallel manner: they quantify abdominal sounds independently for each abdominal region and no propagation is taken into account. Two approaches were proposed by Craine *et al.* [7], who perform source localization by triangulation, and by Dimoulas *et al.* [19], who use a more elaborated decision tree adapted to their hierarchical segmentation technique. The first one is inaccurate, because of the high anisotropy of the propagation environment, while the second one is inapplicable in our detection and segmentation framework. In fact, the technique that we proposed in [17] reduces to what Dimoulas *et al.* call closest point of approach (CPA; [19]); indeed, the simplest hypothesis and, in the actual state of knowledge, the most accurate, is that the recorded sounds are louder when the stethoscope is placed closer to their origin. Therefore, we have proposed a six-region partition of the abdomen, as indicated in Fig. 1. For each sound, we check its maximum amplitude (acoustic

intensity) on each of the stethoscopes that acquired it, and its origin is placed inside the region indicated by the greatest value.

III. DATA ANALYSIS METHOD

Our first proposals for long-term monitoring, based on a set of activity indexes, were made in [12] and [13]. This paper proposes a different phonoenterogram characterization, directly based on the most significant physiological indexes instead of principal components. Therefore, the findings are directly exploitable by clinicians: median values for several physiological indexes are given for different abdominal regions and for different postprandial time intervals.

A. Feature Extraction

Several empirical activity indexes are proposed in the literature: number of sounds by time interval [1], [5], [7], [11], [33]–[35], the sounds duration, energy, power or amplitude integrated over a period of auscultation [2], [3], [5], [6], [33]–[35], sounds main frequency [5], [34], and silence between sounds duration (integrated or averaged over time) [6], [7], [33], [35]. The most commonly considered time interval is the minute, which corresponds to the range of clinical auscultation duration by region. Summarizing, we have considered in our study nine activity indexes, evaluated for each channel and for each minute of recording: the number of sounds (N_m), the total energy (E_m), the total duration of sounds (D_m), the median energy of sounds (E_μ), their median duration (D_μ), their median power (P_μ), their median main frequency (f_μ), their median acoustic intensity (amplitude) (I_μ), and the median duration of silence periods between sounds ($D_{s,\mu}$).

Each minute of recording can then be represented as a point in the 9-D space obtained from the nine activity indexes. Considering our database, we have 14 112 such points, representing 168 min for each of the six regions of the 14 patients. Interpreting all this information reveals to be difficult because of the high dimension of the representation space and, furthermore, because of the probable redundancy of the nine features.³ To diminish the variable redundancy, and thus, the dimension of the representation space, we propose a guided feature-selection step based on a correlation/principal component analysis (PCA) analysis: after PCA, the first four principal components c_1 – c_4 were retained, as they describe more than 80% of the variance. Next, instead of projecting the data onto the reduced principal component space, the original features that are the most correlated with these first four principal components were retained: I_μ , N_m , f_μ , and D_μ (correlated, respectively, to c_1 – c_4 , at least 0.7). We discarded redundant variables as D_m , highly correlated with N_m (0.88), E_μ , and P_μ , highly correlated between them (0.80) and with I_μ (0.67, respectively, 0.68), E_m and $D_{s,\mu}$, uncorrelated with any of the principal components. The first three retained features are almost orthogonal (the maximum correlation coefficient among them is smaller than 0.2), while the last

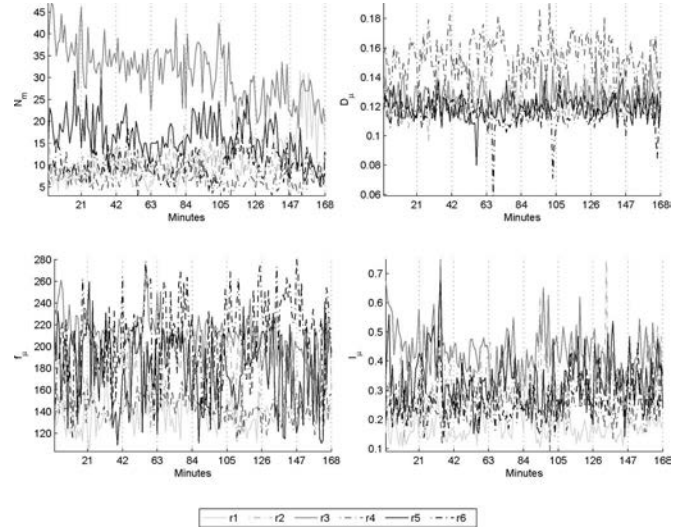


Fig. 6. Evolution of the four selected variables (N_m , D_μ , f_μ , and I_μ) during 168 min for the six regions (median values over the 14 volunteers).

one (D_μ) is a little more correlated (0.4 with I_μ).⁴ This approach permits an easier comparison with the literature and, above all, a natural physiologic interpretation.

B. Statistical Data Analysis

The basic hypothesis is that all recordings are acquired in similar conditions, i.e., after a standardized meal and from a normal population, without particular digestion types (diseases and nutritional habits). The obtained analysis database consists of $14 \times 6 \times 168 = 14\,112$ points (minutes of phonoenterogram) in a 4-D feature space (I_μ , N_m , f_μ , and D_μ).

We recall that the aim of this paper is to determine if the processed phonoenterograms can be used to evaluate differences among different physiologic conditions (digestion evolution) and/or recording sites (abdominal organs). A first visual analysis can be done by plotting the median values of the four retained variables (over the 14 patients), computed for every minute and every region (see Fig. 6): the displayed graphs seem to indicate differences among regions and time evolution during the digestion, but these differences are more easily seen and quantified for certain variables and/or among certain regions and/or during certain time intervals. Thus, this visual impression must be detailed and confirmed by statistical analysis: are the regions or the minutes significantly different? Are these regional differences significant all along the recording? If we consider a particular recording site, is the time evolution significant? These questions will be addressed for all retained variables.

A very critical issue, which can lead to erroneous interpretations, is the experimental design, which must take into account the nature of the analyzed data.

First of all, as the variables (activity indexes) are not Gaussian, nonparametric statistical tests must be used. Different

³We have proposed PCA in [12] and [13] to reduce the number of retained features and to decorrelate them.

⁴All the p -values for the correlation coefficients presented here are highly significant ≈ 0 . This is consistent with the very high amount of data, as for every variable, we have more than 14 000 measures.

ANOVA-like nonparametric tests have been developed and compared in the literature [36]–[40], and it is generally accepted that rank transforming the data (i.e., taking ranks, instead of actual values) can provide robust solutions. This rank transformation can be done in different ways: either 1) globally on the whole data; 2) after aligning the data to eliminate the influence of one of the factors (i.e., subtraction of lines means before testing for column differences, for example); or 3) after ranking separately by factors (i.e., ranking the values on each line separately, instead of ranking the whole data matrix). Intuitively, rank alignment 2) applied on the third factor (patients) will normalize the volunteers by considering equal means, while the separate ranking 3), known as Friedman test, provides almost the same effect, but normalizes both the means and the variances of the patients.

Second, the previous questions have to be translated into a statistical methodology, applied separately and successively for each variable (I_μ , N_m , f_μ , and D_μ).

1) *Gross Analysis*: Perform separate one-way Kruskal–Wallis (KW) tests (equivalent to ANOVA on not aligned ranks [36]) to assess differences among regions considering as replicates all values for a given region, regardless of the patient and minute (respectively, among minutes, considering as replicates all values for a given minute, regardless of the region and patient).

2) *Global Analysis*: The previous simple approach eludes the possible influence of the recording site on the time evolution and of the recording moment on the regional activity. In fact, a more complex design should take into account the three variable factors of the dataset: the regions, the minutes, and the patients. Still, the three factors do not have the same nature: we are interested in differences among regions and among minutes, but not among patients, as our starting hypothesis was that they are all issued from the same healthy population. Nevertheless, we should take into account the interpatient variability when testing for differences among regions and/or minutes. In this design, the third factor is what is called a random factor, and a three-way test with two fixed factors (six regions and 168 min) and a random factor (14 patients) should be performed. Then, perform then a three-ways ANOVA on ranks (not-aligned), with two fixed factors and one random, to test for differences among regions, among minutes, and for possible *interactions* between them. This last term is very critical, because if interaction exists, one should consider separate sets of data by region (respectively, by minute) and make a “fine analysis” as described next.

3) *Fine Analysis*: If interactions are high, Zar [36] recommends to test only for differences between individual cells. This approach would be fastidious and useless: even if the difference is significant, what information could we extract by knowing that a particular minute recorded in a particular region is different from another minute recorded elsewhere? A midpoint solution is to group cells by “families” and test for differences among them: are the regions different, tested minute by minute? Are the minutes different within a particular region (i.e., is there a significant time evolution of the considered activity index for a given region)? This approach implies separate two-way ANOVA on ranks: we only consider data issued from one of the levels of a given fixed main factor, and perform the test according to the

other fixed main factor and the random one. For example, we could consider all regions recorded during a given minute and perform a two-way analysis with one fixed factor (regions) and one random factor (patients). The previously defined 3-D matrix will then split in several 2-D matrices. For each of the 168 min, matrices having six lines (regions) and 14 columns (patients) will be obtained (a similar approach leads to 168×14 matrices for each of the six regions).

A more robust alternative is possible: separate ranking by factors (leading to Friedman test, implemented here using the statistic given by [36] for repeated measures), leads to a reduction of the interaction, and therefore, should be used if the first solution (ANOVA on ranks) reveals a high degree of interaction. Again, this analysis is made for each of the 168 min to test for differences among regions; a similar approach is implemented after considering separate sets of data for each region, to test for differences among minutes.

One final issue before presenting the results. The described tests allow to check for differences among *several* groups, but not between *two* particular groups: they provide the information that at least two groups are different, without indicating which. Multiple comparisons procedures [36], [37] must be used to verify this point. Some authors [36] recommend to use them only if global ANOVA-type tests indicate significant differences, while others [41] have the completely opposite opinion. Among these tests, the current approach on ranked data (after KW or Friedman) is the Nemenyi nonparametric multicomparison [36], which we used when these tests were applied. The results of multiple comparisons are presented, as suggested by [36], by underlining together similar groups (not significantly different). For example, $\underline{X_1 X_2 X_3 X_4}$ signifies that X_1 is different from X_3 and X_4 , but is similar to X_2 , which is similar to X_3 also, and so on. As seen in this example, a current problem when using multiple comparisons is their transitivity. We decided to include it in our interpretation of the results: if X_1 is similar to X_2 and X_2 is similar to X_3 , then X_1 is similar to X_3 . In our example, everything is similar, so we will rather note this as $\underline{X_1 X_2 X_3 X_4}$ and we will say that X_1, X_2, X_3 , and X_4 are found similar after a transitive multiple comparison. Unless explicitly stated, all multiple comparison results in this paper are transitive. This choice might seem to restrictive, but, having in mind the actual state of knowledge on the abdominal sounds, we have decided to favor statistical validity of our findings with the risk of loosing more subtle and detailed interpretations.⁵

IV. EXPERIMENTAL RESULTS

Fig. 6 presents the time evolution for the retained variables and for each region. Median values computed over the 14 volunteers are displayed. As one can see, the third region seems richer in sounds than the others, especially than the first one (see Fig. 1 for positioning). This difference is present for the first part of the recording, but it attenuates at the end. Moreover, as the dispersion of the patients around median values is not displayed, we cannot visually appreciate if this difference is significant or

⁵For example, groups $X_1 X_2$ and $X_3 X_4$ could be considered different.

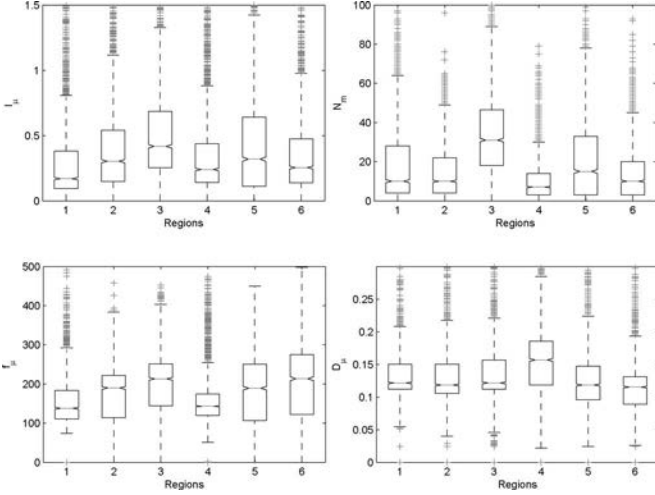


Fig. 7. Box plots of the four variables (I_μ , N_m , f_μ , and D_μ) for six regions (all minutes included). The medians for each region are represented with their confidence intervals (notches) to facilitate multiple comparisons. Box limits are at 25 and 75 percentiles (i.e., 50% of the minutes are “inside” the box), while “+” signs represent outliers (minutes situated outside the limits defined by extending the box, in both directions, by 1.5 its size).

if it is masked by a high patient intervariability. This is the role of the statistic test, and their results are presented hereafter.

A. Gross Analysis

A possible quantification of the differences among the main factors (regions and minutes), completely ignoring any possible interactions, can be done by KW tests. As expected, minutes cannot be separated, all p values are superior to 0.05. On the contrary, the regions are significantly different for all of the four considered variables.

Still, the outputs of the KW tests indicate that a difference exists, without specifying which precise regions are different. Multiple comparisons using the Nemenyi test were then performed and the results can synthetically be presented using the underlining notation introduced in the previous section. According to the four activity indexes, the regions show the following differences: for the sound intensity I_μ : $r_3 r_2 r_5$ $r_6 r_4 r_1$, for the number of sounds N_m : $r_3 r_5$ $r_1 r_2 r_6 r_4$, for the median frequency f_μ : $r_3 r_6$ $r_5 r_2$ $r_4 r_1$, and for the median sound duration D_μ : $r_4 r_3 r_1 r_2 r_5 r_6$.

Synthetically, the third region emits more sounds than the others, with higher frequencies and intensities, while the fourth region has longer sounds, but very few. The sound intensity cannot be used to distinguish between the second and fifth regions, nor the number of sounds between the first, second, and sixth. Different other interpretations are left to the reader, but we remind that no interaction is taken into account here, and therefore, only very global and approximate statements can be made concerning the differences among regions and the absence of difference among sequences (see Fig. 7).

The previous multiple comparisons results confirm the visual analysis suggested by Fig. 6: if the auscultation is performed during a long enough period, the different abdominal regions

have statistically distinguishable activity. All of the selected features can be used, and the regions can generally be sorted according to these features (although the second region, for example, cannot be individually separated from the others).

B. Global Analysis

A more complete approach is a three-way ANOVA with two fixed factors (regions and minutes) and one random factor (patients), performed after rank transformation on each of the four variables. This step permits to evaluate the interactions: if they are not present, the differences revealed by this method would be sufficient for the phonoenterogram analysis.

For f_μ , the obtained p -values indicate very high levels of interaction among all factors, and therefore, no analysis on main factors can be performed. For I_μ and D_μ , very high interactions exist between regions and patients, and between minutes and patients, but no significant value appears for regions–minutes interaction ($p = 0.26$ and $p = 0.36$, respectively). Still, both main factors have a high interaction with the patients, and therefore, interpreting main factors might be misleading for these variables also. For N_m , the results are similar, with high interactions between regions and minutes, and between minutes and patients. Ignoring the interactions, it seems that all variables permit to detect significant differences among regions ($p = 0.005$, $p = 0.002$, $p = 0.0005$, and $p = 0.0007$ for I_μ , N_m , f_μ , and D_μ , respectively), but not among minutes ($p = 0.97$, $p = 0.99$, $p = 0.65$, and $p = 0.73$).

C. Fine Analysis

As described in the previous section, in case of interaction, data are considered separately. A first option is to test for differences among regions for each minute to confirm and detail the results presented for the gross analysis (see Section IV-A). The second option is complementary: consider regions separately and test for differences among minutes.

1) *Regional Activity Distribution During Digestion*: This section aims to find if the regions can be considered statistically different after a 1-min auscultation, and if so, which minute after the meal is the most appropriate. Unfortunately, testing for differences among regions for a given minute (Friedman test) does not give any significant result: 1 min of auscultation is not sufficient to distinguish between abdominal regions, regardless of the activity index. This result seems to contradict the information from Fig. 6: it seems quite clear that, for N_m , for example, the third region is higher than the others for the first part of the recording. The same observation can be made for f_μ (regions r_1 and r_4 lower than r_6 around minute 120) or for D_μ (region r_4 higher than r_6 around minute 70). On the other hand, the curves from Fig. 6 show certain natural trends, which seem to indicate that successive minutes belong to similar physiologic conditions. Therefore, we have decided to concatenate several minutes to form sequences and to test further on for differences among regions by sequence (instead of by minute). Two solutions are possible: either recompute the activity indexes for the new time interval, or consider the minutes belonging to a sequence as statistical replicates (i.e.,

representative measures for the given sequence). We adopted the second solution; on one hand, it preserves the physiological activity indexes defined in the literature and used for the previous results and, on the other hand, it improves the statistic tests reliability.

Different lengths for the tested sequences (analysis windows) have been considered, from 2 to 42 min. As a first approach and to ease the interpretation, we did not consider sliding windows, but contiguous and disjoint (i.e., 84–4 different sequences). It is clear that, for long sequences, the time position (when to analyze) is less precise, as the analysis comes close to the gross KW tests. Moreover, as the activity indexes are nonstationary (see Fig. 6), long sequences might mask regional differences that are more important during certain digestion phases. Therefore, in our opinion, the optimal length of a sequence should be a compromise: long enough to obtain statistical significance, but as short as possible, to have a good time resolution and stationary signals. Still, as no *a priori* knowledge exists and having these considerations in mind, we present here the different obtained results, with a particular focus on sequences having 21-min length, considered optimal.

For sequences having a 2-min length, the results start to confirm the gross KW observations. For example, for the N_m variable, the Friedman test has a significant p -value for almost all sequences (i.e., there are differences among regions) and Nemenyi multiple comparisons indicate that the third region r_3 produces more sounds than the others. In particular, a 2-min auscultation during the first 10 min after the meal, as well as between minutes 60 and 80, should permit to order the regions: r_3 is the richest (and significantly different), followed by r_5 .

The number of sounds by minute N_m is not the only variable permitting to distinguish among regions: D_μ indicates that the fourth region r_4 produces significantly longer sounds around minutes 60 and 120.

These findings are confirmed by 3- and 5-min sequences. For example, for 5-min sequences, I_μ indicates that r_3 is significantly louder than the others during the first 10 min, and between minutes 90 and 110. The sound duration D_μ is generally longer for r_4 , and this is constantly and significantly evident 2 h after the meal (minutes 115–125).

Longer sequences reinforce the presented results. A particularly interesting case is obtained for 21-min length sequences, which split the recording into eight equal parts: the differences given by the statistical tests have a degree of significance similar to those obtained for the whole length. For all the sequences, the loudest region (I_μ) is r_3 (corresponding to the ileocecal valve, i.e., gut–colon junction) and the most quiet is r_1 (stomach or upper colon). Transitive multiple comparisons using Nemenyi tests allow individual separation of r_3 from all other regions for all sequences. Region r_1 (the most quiet) can also be separated according to these tests during the first hour (sequences 1–3). Globally, *the third region is significantly louder and the first region is significantly quieter than the others at the beginning of the digestion, and the third region remains so during all the recording period.* Again, this conclusion gives a statistic confirmation to the visual impression from Fig. 6, where these

TABLE I
REGION ORDERING AND MULTIPLE COMPARISONS BY SEQUENCE (21-MIN LENGTH) AND ACTIVITY INDEX

Sq.	I_μ	N_m	f_μ	D_μ
s1	<u>r3r5r6r4r2r1</u>	<u>r3r5r6r2r4r1</u>	<u>r3r5r6r2r4r1</u>	<u>r4r3r1r5r2r6</u>
s2	<u>r3r5r2r6r4r1</u>	<u>r3r5r6r2r1r4</u>	<u>r3r6r5r2r4r1</u>	<u>r4r3r1r2r6r5</u>
s3	<u>r3r2r4r5r6r1</u>	<u>r3r5r2r6r1r4</u>	<u>r3r6r5r2r1r4</u>	<u>r4r3r2r1r6r5</u>
s4	<u>r3r5r2r4r6r1</u>	<u>r3r5r2r6r1r4</u>	<u>r6r3r5r2r4r1</u>	<u>r4r2r1r3r5r6</u>
s5	<u>r3r5r2r4r6r1</u>	<u>r3r5r2r1r6r4</u>	<u>r3r6r2r5r4r1</u>	<u>r4r3r1r2r5r6</u>
s6	<u>r3r5r6r2r4r1</u>	<u>r3r5r6r2r1r4</u>	<u>r6r3r5r2r4r1</u>	<u>r4r3r1r2r5r6</u>
s7	<u>r3r2r6r5r4r1</u>	<u>r3r1r5r2r6r4</u>	<u>r6r3r5r2r1r4</u>	<u>r4r1r3r2r5r6</u>
s8	<u>r3r2r6r5r4r1</u>	<u>r3r1r5r2r6r4</u>	<u>r6r3r5r2r1r4</u>	<u>r4r3r2r1r5r6</u>

differences among regions are more or less visible during the recording.

Almost similar conclusions can be obtained for the second variable (N_m). It is still r_3 , which is the richest in sounds, while the poorest is r_4 (lower central abdomen), except for the first sequence, when r_1 has the lowest number of sounds. Multiple comparisons are more significant at the beginning and at the middle of the digestion, than at the end (preprandial period): r_3 is significantly different from all the others from the first sequence until almost 2:30 h after the meal (first seven sequences), but it cannot be distinguished from r_1 (stomach) for the last 21 min (when most of the volunteers were hungry, with their stomach gurgling). During the last four sequences, the fourth region r_4 was also significantly poorer.

From a frequency f_μ point of view, the regions are significantly different during all sequences. *The third and the sixth regions are the highest in frequency (r_3 during the first hour and r_6 during the last hour), while r_4 and r_1 are the lowest (r_1 during sequences 1, 2, 4–6, and r_4 during sequences 3, 7, and 8).* Nevertheless, according to Nemenyi tests, r_3 is significantly higher than all the others only during the first 21 min ($r3r5r6$, $r2r4r1$) and r_6 is significantly higher only during sequence 7 ($r6r3r5r2$, $r1r4$).

The analysis performed on D_μ shows that regions are significantly different according to both Friedman and ANOVA on ranks tests all along the recording, except for the last 21 min, when ANOVA output becomes insignificant. *The fourth region (gut) has the longest sounds during all the digestion, and it is significantly different from all others (Nemenyi test) for the first approximately 2:30 h after the meal (sequences 1–7). The shortest sounds are generated in regions 5 and 6, but they are significantly different only at the middle of the digestion (sequence 3: $r4r3r2r1$, $r6r5$, sequence 4: $r4r2r1r3r5r6$, and sequence 5: $r4r3r2r1r5r6$).*

In order to enforce the statistical validity of the results and to ease the lecture, all the previous multiple comparisons were *transitive*. The results of the nontransitive multiple comparisons are not detailed here, but a synthetic view is shown in Table I, which completely presents the interregion differences for a sequence length of 21 min. All multiple comparisons (for the four variables and the eight sequences) are represented by underlining similar regions.

2) *Activity Time Evolution by Region:* Following the same approach, we present here a detailed analysis by region, the goal being to separate among minutes (or sequences) inside each

region. In other words, we attempt to propose a phonoenterogram segmentation based on statistical characteristics.

As in Section IV-C1, a first approach considers equal-length sequences and varies this length in order to find the necessary (minimal) value for a reliable statistical analysis. Keeping this duration small, allows us to preserve a good time resolution for a possible segmentation of the phonoenterograms in digestion phases; indeed, for each variable, *consecutive similar* time sequences could be associated, according to the results of the statistical tests, to define physiological digestion phases, while the frontiers between two phases would be placed between two *consecutive different* sequences.⁶ It is clear that as the (constant) length of the sequence increases, the resulting segmentation becomes suboptimal, both because of the phonoenterogram “subsampling” and its nonstationarity. Nevertheless, these segmentation results lead to a first approximation of the abdominal activity by piecewise constant functions: curves from Fig. 6 could be approximated by constant fixed-length segments. Similar level segments (i.e., not significantly different according to the tests) can then be concatenated to define a longer phase, the obtained result being a first segmentation of the phonoenterogram in statistically different digestive phases.

Clearly, different other approaches can be adopted. For example, variable length sequences could be segmented directly on the curves from Fig. 6, based on some consistency criteria (trend changes, piecewise linear regression), and the resulting digestive phases could be compared among them by statistical tests to assess the validity of the proposed segmentation. A third method could propose physiologically defined phases, according to the actual medical knowledge on the digestion (phases of the migrating motor complex, for example), with again an *a posteriori* statistical validation. Both these last two approaches might possibly offer a more precise segmentation of the digestion, but on the other hand, they need a consecutive statistical validation that risks to concatenate them if the necessary level of significance is not reached. In our opinion, implementing statistical tests to check for significant differences among trends (or slopes of piecewise linear regressions) exceeds the aim of this paper and the actual state of knowledge on the abdominal sound activity. Therefore, in this paper, the first described method (constant piecewise segments) is only implemented, although less precise, it directly offers the needed statistical significance.

As expected, sequences of 1-min length cannot be significantly distinguished regardless of the region or the activity index. We adopted the same approach, concatenating the minutes into longer equal size contiguous sequences and testing for differences among them. As argued in the previous paragraph, this leads to an approximate segmentation of the phonoenterogram (by variable, for each region).

The shortest sequences that can be differentiated last for 15 min (11 sequences for the first 165 min), but this is only possible for one variable (N_m) and one region (r_1). More pre-

cisely, Friedman test gives $p < 0.01$ and multiple comparisons yield the following order $\underline{s_{11} s_{10} s_9} \underline{s_7 s_8 s_6 s_3 s_2 s_1 s_5 s_4}$, which means that during the last 45 min (i.e., starting 2 h after the meal), the region r_1 is significantly richer in sounds than during the first 2 h.

Increasing the sequence duration improves the results of the tests. For 21-min sequences (eight sequences), several regions display significant time evolution, mainly concerning the number of sounds N_m . Multiple comparisons with Nemenyi test permit to individually distinguish digestion phases for two regions: for r_1 , the last sequence (sequence 8) is the richest in sounds, followed by sequence 7 ($\underline{s_8 s_7 s_6 s_5 s_1 s_2 s_4 s_3}$); for r_3 , the evolution of the number of sounds follows an inverse path: the richest is the first sequence, immediately after the meal, and the poorest is the eighth, when the digestion is probably finished and the volunteers are right before their next meal ($\underline{s_1 s_2 s_3 s_4 s_5} \underline{s_6 s_7 s_8}$). It is quite remarkable that these evolutions show constant natural trends: the stomach makes more sounds when empty (i.e., when the person is hungry), while the lower right abdomen (end of the gut, ileocecal valve) is very active at the beginning of the digestion and its activity decreases constantly until the end.

Finally, splitting the recording in only four sequences having 42-min length each, all variables become significant, depending on the region. For r_1 , the last 42 min are the richer in sounds and the loudest (for N_m , we have $\underline{s_4 s_3 s_1 s_2}$, while for I_μ , we have $\underline{s_4 s_3 s_2 s_1}$), although the sound intensity is not significantly higher according to Nemenyi test, except compared with s_1 (first 42 min). The number of sounds permits to establish significant time evolutions also for regions 2, 3, 4, and 5 ($r_2 : \underline{s_2 s_3 s_4 s_1}$, $r_3 : \underline{s_1 s_2 s_3 s_4}$, $r_4 : \underline{s_2 s_1 s_3 s_4}$, and $r_5 : \underline{s_3 s_1 s_2 s_4}$). Frequency evolution can be observed for $r_1 : \underline{s_2 s_1 s_4 s_3}$, $r_4 : \underline{s_2 s_1 s_3 s_4}$, and $r_6 : \underline{s_4 s_2 s_3 s_1}$, and median sound duration for $r_1 : \underline{s_4 s_3 s_2 s_1}$ and $r_4 : \underline{s_3 s_2 s_1 s_4}$. Although not always obvious, some natural trends can be detected using these long-duration sequences. The number of sounds N_m seems a valid indicator of the normal digestion evolution for almost all regions: it constantly increases for the stomach (r_1), it constantly decreases for the ileocecal region (r_3), and it has a similar evolution for the preceding segment (lower abdomen r_4). The frequency is higher during the first half of the digestion both for r_1 and r_4 . This last observation is also confirmed by a gross analysis: KW and Nemenyi tests for sequence differences, regardless of the region and of the patient, indicate that s_2 (second quarter of the recording) has significantly higher frequencies than the other periods: $\underline{s_2 s_1 s_4 s_3}$.

Interestingly enough, the segmentations resulting from different sequence lengths confirm each other in most of the cases, or at least they are complementary, for example, taking the first region r_1 and variable N_m , all considered sequences (15, 21, or 42 min) lead to the conclusion that the last part of the phonoenterogram (40–45 min) is statistically different from the previous sequences, with complementary information given by the last two analysis (21 and 42 min).

A synthetic presentation of the intersequence differences, including all the multiple comparisons results, is presented in Table II for 21-min-length sequences.

⁶Moreover, the shorter the necessary duration for a reliable statistical analysis, the easier the clinical implementation. Even if, for the moment, it is speculative and further tests are needed, this approach should permit to suggest clinical guidelines for the abdominal auscultation.

TABLE II
REGION ORDERING AND MULTIPLE COMPARISONS BY SEQUENCE (21-MIN LENGTH) AND ACTIVITY INDEX

Rcg.	I_{μ}	N_m	f_{μ}	D_{μ}
r_1	<u>s8 s4 s6 s7 s5 s3 s2 s1</u>	<u>s8 s7 s6 s5 s1 s2 s4 s3</u>	<u>s3 s4 s1 s8 s2 s5 s7 s6</u>	<u>s7 s8 s6 s5 s4 s3 s2 s1</u>
r_2	<u>s8 s3 s7 s2 s4 s5 s6 s1</u>	<u>s4 s6 s3 s5 s7 s8 s2 s1</u>	<u>s8 s2 s5 s4 s3 s6 s7 s1</u>	<u>s8 s7 s4 s3 s2 s6 s5 s1</u>
r_3	<u>s1 s5 s3 s2 s8 s6 s4 s7</u>	<u>s1 s2 s3 s4 s5 s6 s7 s8</u>	<u>s1 s4 s3 s5 s7 s6 s2 s8</u>	<u>s8 s7 s4 s3 s2 s6 s5 s1</u>
r_4	<u>s3 s4 s1 s2 s5 s6 s8 s7</u>	<u>s4 s3 s1 s2 s5 s7 s8 s6</u>	<u>s1 s4 s3 s2 s5 s8 s7 s6</u>	<u>s2 s6 s3 s4 s5 s1 s7 s8</u>
r_5	<u>s2 s1 s4 s7 s6 s8 s5 s3</u>	<u>s5 s4 s1 s2 s3 s6 s7 s8</u>	<u>s1 s4 s3 s2 s5 s8 s7 s6</u>	<u>s1 s2 s6 s5 s4 s7 s8 s3</u>
r_6	<u>s8 s7 s3 s6 s1 s2 s5 s4</u>	<u>s6 s3 s7 s2 s4 s8 s5 s1</u>	<u>s7 s4 s6 s8 s3 s5 s1 s2</u>	<u>s2 s8 s7 s3 s6 s1 s5 s4</u>

V. CONCLUSION AND FUTURE RESEARCH

This paper addresses two main issues: the abdominal sounds processing methodology and their detailed statistical analysis.

Several methodological signal processing steps were proposed and/or improved, and the resulting chain was employed to extract physiologically meaningful data from the long-term multichannel phonoenterograms. The proposed solution is effective, although an interesting perspective research could be the comparison of the different other signal processing methods developed in the recent literature for abdominal sound analysis. However, the processing steps proposed in this paper proved to be reliable enough to furnish statistically consistent information, analyzed in the second part of this paper.

Two types of analysis were performed, aiming to check if and under which conditions abdominal auscultation can furnish statistically reliable data on the normal digestion, both in terms of localization and time evolution.

According to our results, abdominal activity in different regions can be distinguished using abdominal auscultation. It seems that, to differentiate between regions, rather short-term auscultation (3–5 min) can be sufficient, especially (but not only) when this auscultation is performed immediately after the meal. For example, for normal digestion, the third considered region r_3 (lower right abdomen, ileocecal valve) should be louder, should emit more sounds, and have higher frequencies. Approximately 2 h after the meal (digestion final phases), the sounds emitted in the lower central abdomen r_4 are significantly longer than those from the other regions. Of course, future validation on healthy and pathologic cases is needed, but present results indicate that these findings consistently describe normal functioning of the abdominal tract. A comparative view of all results suggests some interesting information for clinical auscultation: it seems that the most informative regions, at least for analyzing normal digestion, are r_1 , r_3 , and r_4 (stomach, ileocecal region, and gut region); the most effective activity index is the number of sounds N_m , although complementary information is carried by the other indexes; finally, better results can be obtained by an immediately postprandial auscultation, although later phases are also informative, especially if the auscultation is longer.

A more difficult issue is the analysis of the digestion evolution over time using the selected physiological activity indexes. Although some trends can be detected, and thus, individual minutes or short sequences of auscultation seem different at the beginning and at the end of the digestion process (especially when counting the sounds emitted by the stomach and by the lower right abdomen), we were not able to prove this differ-

ence statistically. Even if digestion evolution cannot be clearly evaluated by realistic (short-time) clinical auscultation, long-time phonoenterograms can do it. Indeed, considering longer auscultation sequences (unrealistic in clinical environment, but possible using an automatic system), these trends can be detected from the recorded data and they become significant, not only considering the number of emitted sounds, but also in duration, frequency, and intensity. This point also needs further validation, and we are confident that a more extensive database can improve the statistical reliability of our results.

An important point not completely addressed in this paper is the length of the auscultation sequence needed to distinguish among regions or among sequences themselves. Our current proposal was to consider equal-length sequences, which is a coherent approach from a statistical point of view: estimation made over populations having similar sizes have similar properties (confidence intervals), and further comparisons are facilitated. Nevertheless, a physiologically justified approach would consist in a previous segmentation of the time evolution of the activity indexes, in order to detect possible natural digestion phases, which can be further tested for statistical differences using a more elaborate test methodology. Hopefully, this approach should permit to propose and confirm a finer segmentation of the digestion phases and will be addressed in a future work.

An important future research direction is the validation of the proposed signal processing and data analysis methodology on a more extensive database and pathological cases, leading to a possible increase of the statistical validity. Still, the results presented in this paper convey statistical evidence that the regional abdominal activity of healthy patients shows a certain structure. More precisely, a time-evolving activity pattern can be established for healthy patients, and one can speculate that changes in this pattern reflect a modified patient state (health, digestion phase, and digestion habits).

For the moment, no pathological case was recorded using the standardized protocol, but a short phonoenterogram of a patient with gastritis was easily distinguished from the others (higher sound intensity and number, especially in r_1). As our method allows a precise analysis of the normal abdominal functioning, we are confident that pathologic recordings can also be characterized. An important problem is the creation of a standard healthy phonoenterogram database, necessary for any further comparative study.

In our opinion, the main conclusion of this paper is that normal (and possibly pathologic) gastrointestinal activity might be analyzed using abdominal auscultation, but this should be done with great care: if the region differences can be assessed

by rather short-time auscultation, and thus, in a clinical environment, digestion evolution evaluation needs longer recording periods, and thus, an automatic tool.

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