

Effect of manipulation of the feet and ankles on postural control in elderly adults

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Abstract

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The purpose of the present experiment was to investigate the effect of a therapeutic 2 manipulation of the feet and ankles on postural control during quiet standing in elderly 3 adults. Seventeen elderly adults stood barefoot on a force platform and were asked to sway 4 5 as little as possible. Within a trial, vision was suppressed by eyes closure. The task was 6 executed in two experimental sessions: before and after a therapeutic manipulation of the foot and ankle. Centre of foot pressure (COP) displacements along the mediolateral (ML) 7 8 and anteroposterior (AP) axes were recorded. For the two experimental sessions, subjects 9 exhibited comparable COP displacements when vision was available and were similarly 10 affected by the suppression of vision. However, when subjects had to adapt to the absence 11 of vision within a 10 s temporal frame, postural behavior became different in the two 12 experimental sessions: The sum of the ML and AP COP displacements increased within the 13 10 s temporal frame before the therapeutic manipulation of the feet and ankles, whereas it remained unchanged after it. These results suggested that the therapeutic manipulation of 14 the foot and ankle allows the elderly adults to partially compensate for the destabilising 15 effect induced by the suppression of vision. 16

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Key words: Manipulation; Foot; Ankle; Balance; Elderly.

Introduction

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Postural control is a particularly complex system involving various sensory and 2 motor components. Among the sensory inputs relevant to the regulation of postural sway, 3 the importance of somatosensory information from the feet and ankles is now well 4 5 established (Dietz, 1992; Fitzpatrick et al., 1994; Meyer et al., 2004a, 2004b). Data 6 supporting this view were obtained through experimental and clinical approaches. Experimental manipulations of somatosensory information from cutaneous, muscles, 7 8 tendons and joints receptors were shown to have an effect on postural control, as evidenced 9 either by cooling (Magnusson et al., 1990), anaesthetising (Thoumie & Do, 1996; Meyer et 10 al., 2004a, 2004b) or stimulating (Kavounoudias et al., 1998, 2001; Maurer et al., 2001) the 11 plantar soles, by vibrating ankle muscles (Kavounoudias et al., 1998; Hay et al., 1996), by applying an ischemic block above the ankles (Fitzpatrick et al., 1994; Dierner et al., 1984), 12 or by changing the characteristics of the supporting surface on which individuals are 13 standing (Redfern et al., 1997; Robbins et al., 1998). Clinically, alteration or loss of 14 somatosensory information from the lower limbs resulting from disease (diabetic peripheral 15 neuropathy) is known to impair postural control (Simmons et al., 1997). Progressive 16 degeneration of sensory inputs from the lower extremities also represents a common 17 clinical finding associated with aging (Kenshalo, 1986; Skinner et al., 1984) and has even 18 19 been identified as an important contributing factor to the occurrence of falls in elderly (Lord et al., 1991; Tinetti & Speechley, 1989). Therefore, it is legitimate to propose that a 20 therapeutic intervention designed to increase somatosensory function of the feet and ankles 21 22 could be of great interest for controlling balance and preventing falls in the elderly. While the benefits of proprioceptive exercises are documented (Gauchard et al., 1999; Sinaki & 23

- Lynn, 2002), it is surprising that there is an absence of data investigating whether and how
 a therapeutic manipulation of the feet and ankles can modify postural control in elderly
- 3 adults.

The purpose of the present experiment was to improve the understanding of the 4 5 contribution of distal lower limb inputs to the control of balance during functional 6 activities. More precisely, it was to investigate the effects of a therapeutic manipulation of 7 the feet and ankles on postural control during quiet standing in elderly adults. Since visual 8 information is known to play an important role in postural control, particularly in elderly 9 (Lord & Menz, 2000; Sundermier et al., 1996), subjects' ability to regulate their postural 10 sway was evaluated while being exposed to an abrupt suppression of visual information, as 11 previously done by others (Hay et al., 1996; Teasdale et al., 1991). It was hypothesised that 12 an "over-activation" of somatosensory information induced by a therapeutic manipulation of the feet and ankles allows the elderly persons to compensate for the destabilising effect 13 of visual suppression. Since the somatosensory system includes various receptors that 14 15 provide information about pressure distribution (cutaneous), muscle tension (Golgi tendon organs), joint angle changes (joint receptors) and muscle length changes (spindles), the 16 intervention involved manual massage of the feet and mobilisation of both the feet and 17 ankles joints. 18

Methods

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17 male elderly adults (mean age = 74.5 ± 9,.6 years; mean body weight = 73.2 ±

12.3 kg; mean height = 165.6 ± 9,3 cm) participated in the experiment. Subjects were

volunteers and gave written informed consent to the experimental procedure as required by

the Helsinki declaration (1964) and the local Ethics Committee. None of the subjects

- presented any musculoskeletal problems, defects in the peripheral sensory system of the
- 2 lower extremities, vascular pathology, neurological disorders or vestibular impairment.
- 3 Finally, all subjects had normal or corrected-to-normal vision.

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Subjects stood barefoot on a force platform, feet joined, and were asked to sway as 4 5 little as possible, with their eyes open. Fifteen seconds into a trial, an auditory stimulus 6 directed the subjects to close their eyes. A trial finished with 10 s of no-vision. When vision 7 was available, subjects were asked to fixate the intersection of a black cross placed onto the 8 white wall distant 1 m in front of them, at the eyes level. When vision was not available, 9 they were asked to keep their gaze in a straight-ahead direction. This task was executed in 10 two experimental sessions (Pre- and Post test). Six 25 s trials were executed for each 11 experimental session, for a total of 12 trials. The duration of an experimental session lasted 6 min, approximately. The Pre-test served as a control session. In the Post-test session, the 12 measurements were performed immediately after a therapeutic manipulation of the feet and 13 ankles. This intervention, widely used by manual therapists (Dufour, 1996), was designed 14 15 to target the somatosensory system of the feet and ankles, using manual massage of the feet and mobilisation of both the feet and ankles joints. 16

The aim of the massage was to enhance local blood circulation and to stimulate cutaneous receptors. Massage technique application involved frictions and glide force pressure of the plantar sole. Mobilisations elicited dorsiflexion and plantar flexion of the mortise joints, eversion and inversion of the subtalar joints, anteroposterior glide, torsion, flexion and extension of the midtarsal joints, anteroposterior glide and rotation of tarsometatarsal joints, anteroposterior glide of intermetatarsal joints, plantar flexion and extension of metarsophalangeal and interphalangeal joints. Manual massage and

- articulation techniques were applied to both the feet and ankles for 20 min. Six 25 s trials were executed for each experimental session, for a total of 12 trials. The duration of an
- 3 experimental session lasted 6 min, approximately.

- A force platform (AMTI model OR6-5-1) was used to measure displacements of the centre of foot pressure (COP). Signals from the force platform were sampled at 200 Hz (12 bit A/D conversion) and filtered with a second-order low-pass Butterworth filter (10 Hz cut-off frequency).
 - CoP displacements (*in millimetres*) along the mediolateral (ML) and anteroposterior (AP) axes were used to estimate a global postural performance before and after the therapeutic manipulation. This measure corresponds to the sum of the displacement scalars over the sampling period. For convenience purposes, these two dependent variables will be referred to as ML and AP COP displacements, respectively. The first 10 sec of a trial were used to allow subjects' stabilisation. COP displacements were analysed over three periods of 4 s, immediately before the suppression of vision (T1), 1 s after the visual transition to prevent from the presumed effect of the visual transition from vision to no-vision (T2) and at the end of the trial (T3). Comparison of these three temporal frames yielded information on (1) the immediate effect of the suppression of vision on COP displacements (T1 vs. T2) and (2) the postural adaptation over time to the absence of vision (T2 vs. T3).
 - Analyses of variance (ANOVAs) were used for statistical comparison of the different conditions. Level of significance was set at 0.05. Post-hoc analyses (Newman-Keuls) were used whenever necessary.

Results

Figure 1 illustrates representative COP displacements across a trial from a typical subject for each of the two Pre (*left panel*) and Post-test (*left panel*) experimental sessions.

5 Insert Figure 1 about here

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Postural control following the suppression of vision

A preliminary analysis consisted in controlling whether the immediate effect of the suppression of vision on COP displacements was similar across the trials performed in the Pre-test session for the temporal frames T1 versus T2. The first three and the last three trials of the Pre-test session were compared using 2 Series (First 3 vs. Last 3 trials) \times 2 Temporal frames (T1 vs. T2) ANOVAs. For both the ML and AP COP displacements, results showed no effect of Series and no interaction of Series \times Temporal frame (Ps > 0.05). This suggested that the immediate effect of the suppression of vision on COP displacements was constant across the Pre-test trials. Thus, data obtained in the Post-test session were not likely to be confounded with a possible effect of training or fatigue.

The purpose of the following analysis was to investigate whether subjects' ability to immediately adapt to the transition from vision to no vision was modified by the therapeutic manipulation of the feet and ankles. 2 Sessions (Pre vs. Post-test) × 2 Temporal frames (T1 vs. T2) ANOVAs with repeated measures on both factors were applied to the data.

Analysis of the ML COP displacements showed a main effect of Temporal frame, 1 2 with smaller ML COP displacements before than immediately after the suppression of vision (F(1,16) = 27.58, P < 0.001). The absence of an interaction of Session × Temporal 3 frame (P > 0.05) showed that the therapeutic intervention did not affect ML COP 4 5 displacements immediately after the visual transition (Figure 2A). 6 Insert Figure 2 about here 7 8 Analysis of the AP COP displacements confirmed a main effect of Temporal frame 9 (F(1,16) = 31.26, P < 0.001) and showed a main effect of Session, yielding smaller AP 10 COP displacements in the Post- than in the Pre-test session (F(1,16) = 8.01, P < 0.05). The 11 absence of an interaction of Session \times Temporal frame (P > 0.05) also showed that the 12 therapeutic intervention did not affect AP COP displacements immediately after the 13 suppression of vision (Figure 2B). 14 To further investigate the persistence of the effect of the manipulation of the feet 15 and ankles, the first three and the last three trials of the Post-test session were compared 16 using 2 Series (First 3 vs. Last 3 trials) × 2 Temporal frames (T1 vs. T2) ANOVAs. For 17 both the ML and AP COP displacements, results showed no effect of Series and no 18 interaction of Series \times Temporal frame (Ps > 0.05). This suggested that the therapeutic 19 20 intervention on COP displacements was constant across the Post-test trials, for 6 min at 21 least. Adaptation of postural control to the absence of vision

A preliminary analysis controlled whether the postural adaptation to the suppression 1 of vision within a 10 s temporal frame was similar in the trials performed in the Pre-test 2 session for the temporal frames T2 versus T3. The first three and the last three trials of the 3 Pre-test session were compared using 2 Series (First 3 vs. Last 3 trials) × 2 Temporal 4 5 frames (T2 vs. T3) ANOVAs. For both the ML and AP COP displacements, results showed no effect of Series (Ps > 0.05), and no interaction of Series × Temporal frame (Ps > 0.05). 6 7 This suggested that postural adaptation to the suppression of vision within a 10 s temporal frame was constant across the Pre-test trials. This further confirmed that data obtained 8 following the therapeutic manipulation were not likely to be confounded with a possible 9 effect of training or fatigue. 10 The purpose of the following analysis was to investigate whether subjects' 11 adaptation to the effect of the visual transition within a 10 s temporal frame was modified 12 by the therapeutic intervention. Two Sessions (Pre vs. Post-test) × 2 Temporal frames (T2 13 vs. T3) ANOVAs with repeated measures on both factors were applied to the data. 14 15 Analysis of the ML COP displacements showed a significant interaction of Session \times Temporal frame (F(1,16) = 6.53, P < 0.05). The decomposition of the interaction into its 16 simple main effects showed that ML COP displacements increased over time in the Pre-test 17 session, with smaller values immediately after the suppression of vision than after 6 s of 18 19 adaptation in No-vision (P < 0.05), whereas they remained unchanged in the Post-test session (P > 0.05) (Figure 2A). 20 Analysis of the AP COP displacements showed a significant interaction of Session × 21 22 Temporal frame (F(1,16) = 5.48, P < 0.05). The ANOVA also confirmed main effects of

- Temporal frame (F(1,16) = 4.53, P < 0.05) and Session (F(1,16) = 11.07, P < 0.01). The
- 2 decomposition of the interaction into its simple main effects showed that AP COP
- 3 displacements increased over time in the Pre-test session, with smaller values immediately
- after the suppression of vision than after 6 s of adaptation in No-vision (P < 0.01), whereas
- 5 they remained unchanged in the Post-test session (P > 0.05) (Figure 2B).
- To further investigate the persistence of the effect of the therapeutic manipulation of
- 7 the feet and ankles, the first three and the last three trials of the Post-test session were
- 8 compared using 2 Series (First 3 vs. Last 3) × 2 Temporal frames (T2 vs. T3) ANOVAs.
- 9 For both ML and AP COP displacements, results showed no effect of Series (Ps > 0.05),
- and no interaction of Series \times Temporal frame (Ps > 0.05). This suggested that the benefits
- of the therapeutic intervention on COP displacements was constant across the Post-test
- trials, for 6 min at least.

Discussion

- The purpose of the present experiment was to investigate the effects of a therapeutic
- manipulation of the feet and ankles on postural control during quiet standing in elderly
- adults. Subjects' ability to maintain a stable upright posture was evaluated while facing
- changes in the availability of visual information before and after the therapeutic
- intervention. Withdrawing visual information forced the subjects to reorganise the
- 19 hierarchy of sensory information since vestibular and proprioceptive inputs became the
- 20 only remaining sources of sensory information available for regulating posture.
- 21 Before and after the therapeutic manipulation, subjects exhibited comparable COP
- displacements when vision was available (temporal frame T1), suggesting that the massage

- and mobilisation of the feet and ankles had no immediate effect on postural stability and/or
- 2 that vision largely compensated for the presumed benefits of a therapeutic manipulation.
- 3 Previous studies showed similar compensations following fatigue of the lower limbs
- 4 (Vuillerme et al., 2001). Similarly, the therapeutic manipulation did not affect COP
- 5 displacements immediately following the visual transition from vision to no-vision
- 6 (temporal frame T2). This absence of effect may be due to the limited impact of the
- therapeutic manipulation with respect to the amplitude of normal body oscillations in the
- 8 absence of vision.

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Interestingly, it is when adapting to this absence of vision within a 10 s temporal frame that the postural behaviour in the two experimental sessions became different (temporal frame T3). After 10 s of adaptation, postural instability still increased in the control session whereas following the therapeutic manipulation subjects seemed able to provide a rapid recalibration and reorganisation of postural control to take into account the new sensory conditions by switching from visual to proprioceptive control. This adaptive mechanism would ensure a stabilisation of subjects' postural behaviour following the withdrawal of vision.

With regard to the hypothesis of a global "over-activation" of somatosensory information induced by the therapeutic manipulation of the feet and ankles, the present results are in line with those of Nougier et al. (1997) when altering somatosensory inputs by means of a foam support surface. In their experiment, postural control in young adults was analysed in different conditions of vision and two conditions of ankle proprioceptive information (normal and altered support surface with a 5 cm thick foam support). When somatosensory information was not altered, as in the Post-test session, young subjects

adapted to the absence of vision. Conversely, when the proprioceptive inputs were altered

by the use of the foam support surface, as in the Pre-test session, subjects showed no

adaptation. Altogether, these results and the present ones demonstrate that the quality of

4 somatosensory information plays a major role in compensating for the absence of vision. In

the present case, the therapeutic manipulation seemed to partially compensate for the

observed alteration of somatosensory information with age (Kenshalo, 1986; Skinner et al.,

1984), by temporarily increasing subjects' sensitivity to these inputs.

In conclusion, the present findings showed that elderly adults can benefit from a therapeutic manipulation of the feet and ankles, even though estimated for a short time, for regulating their postural sway during quiet standing. This suggested that such manipulations may allow people to overcome or compensate for functional difficulties due to age and more generally to disease-related sensory loss. It remains, however, to further investigate the underlying neurophysiological mechanisms and to better locate the sites of these effects. It remains also to further investigate the overall duration of the observed benefits in order to validate the utility of these various manipulations and to better specify the most efficient characteristics of a training/rehabilitation program that would include this kind of manipulation.

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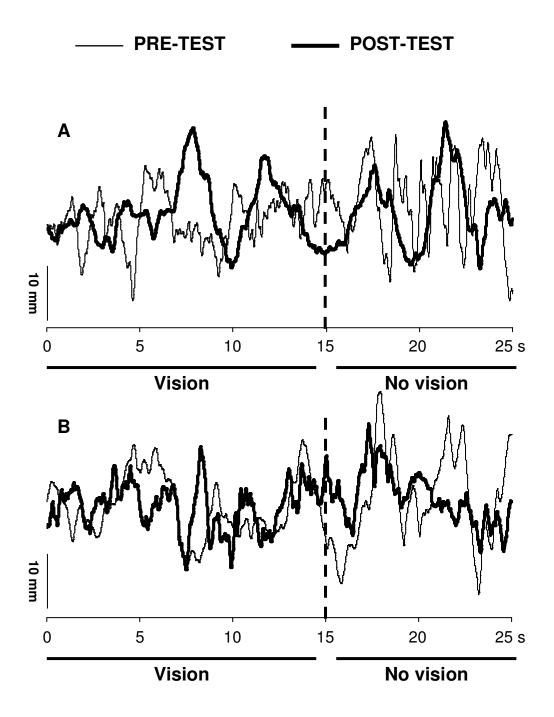
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- fatigue for controlling posture? Neurosci. Lett. 308 (2001) 130-106.

1 Figures captions

- 2 Figure 1. Representative displacements of COP along the mediolateral (A) and
- anteroposterior (B) axis for the two Pre- and Post-test sessions. The dotted lines indicate the
- 4 suppression of vision.
- 5 .

- Figure 2. Mean COP displacements and standard deviation along the two mediolateral (A)
- and anteroposterior (B) axes and for the two Pre and Post-test sessions. The two
- 9 experimental sessions are presented with different symbols: Pre-test (white diamonds) and
- 10 Post-test (black squares).



1 Figure 2

